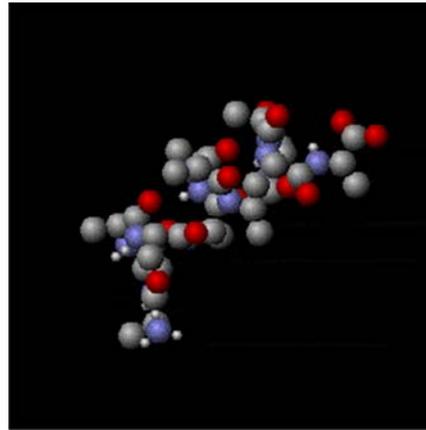


8. Body Temperature

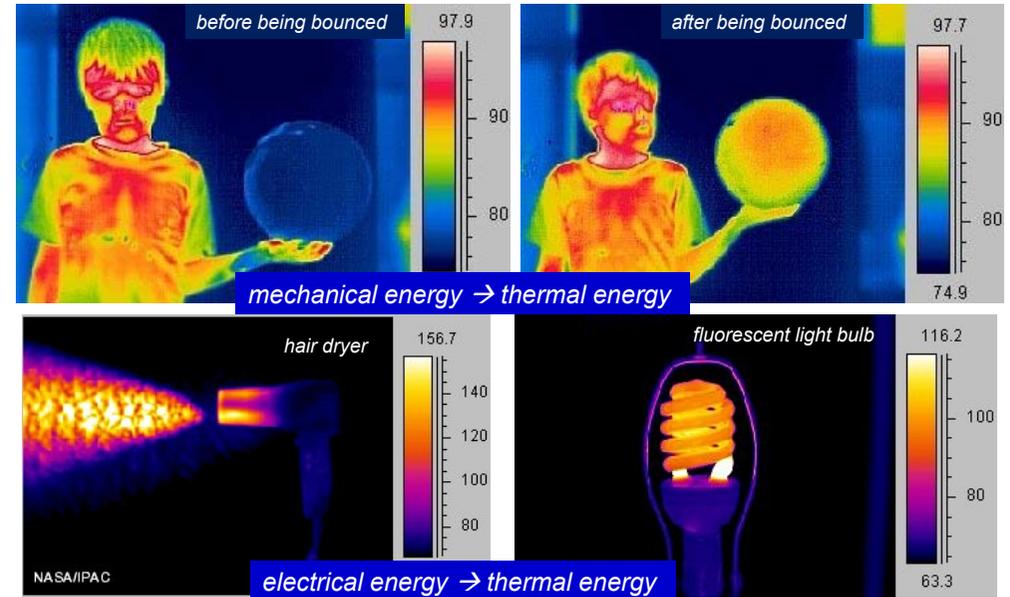
Heat: the total energy of molecular motion in a substance.
Temperature: a measure of the average energy of molecular motion in a substance.

- Body Temperature
- Measurement methods
 - Mercury thermometer
 - Electronic thermometer
 - Infrared thermometer
 - Zero-heat-flow
 - Dual-heat-flux



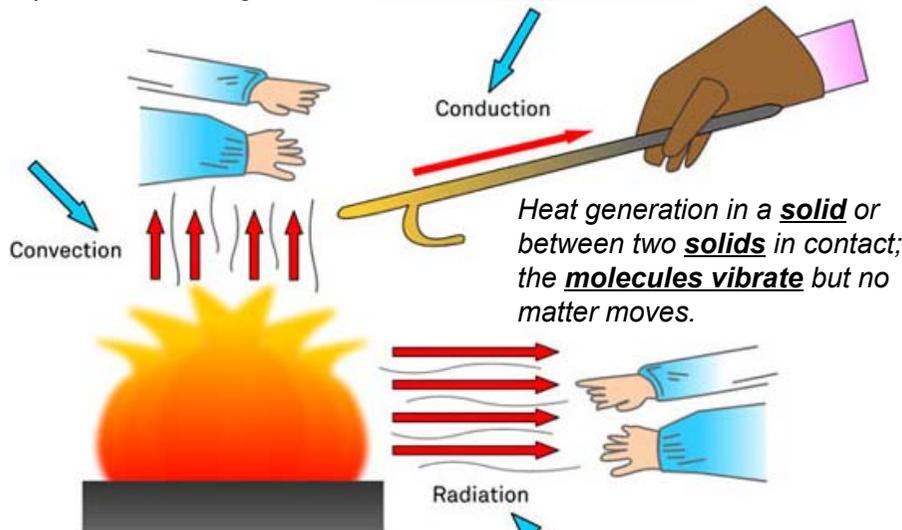
http://en.wikipedia.org/wiki/File:Thermally_Agitated_Molecule.gif

Thermal Infrared Images



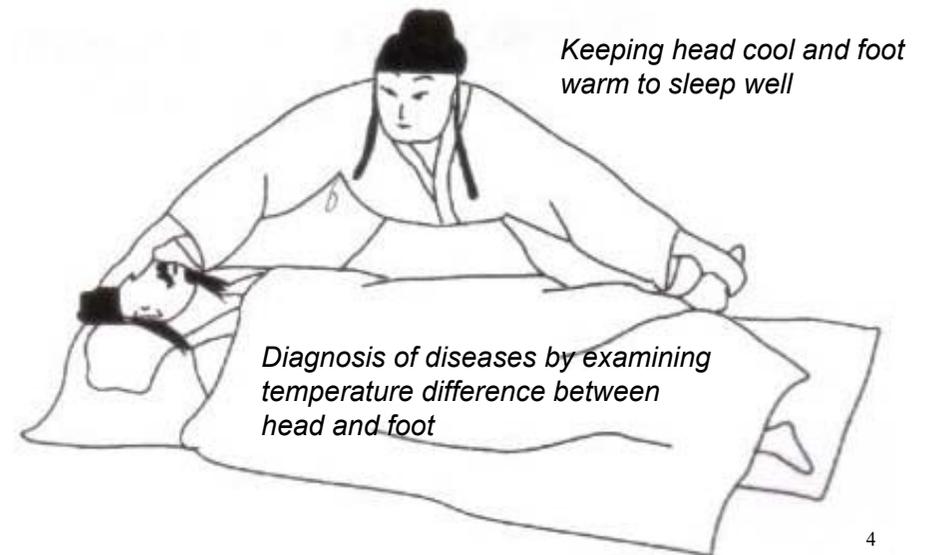
Heat Transfer

Heat generation in a **fluid** (liquid or gas) that is caused by a variation in temperature resulting from the **movement of molecules**.



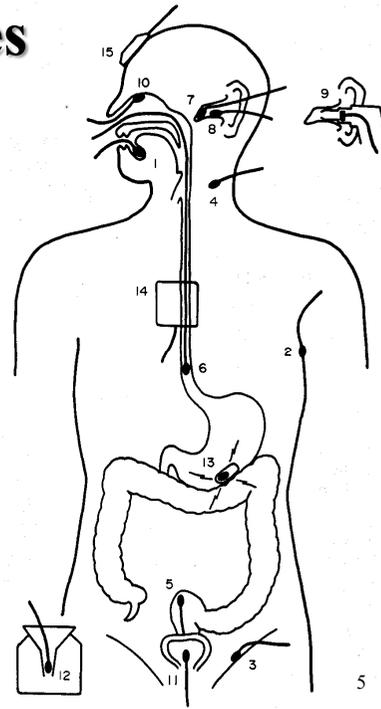
Heat generation in the form of **electromagnetic waves** emitted by a heated body (solid, liquid or gas).

Archaic Method



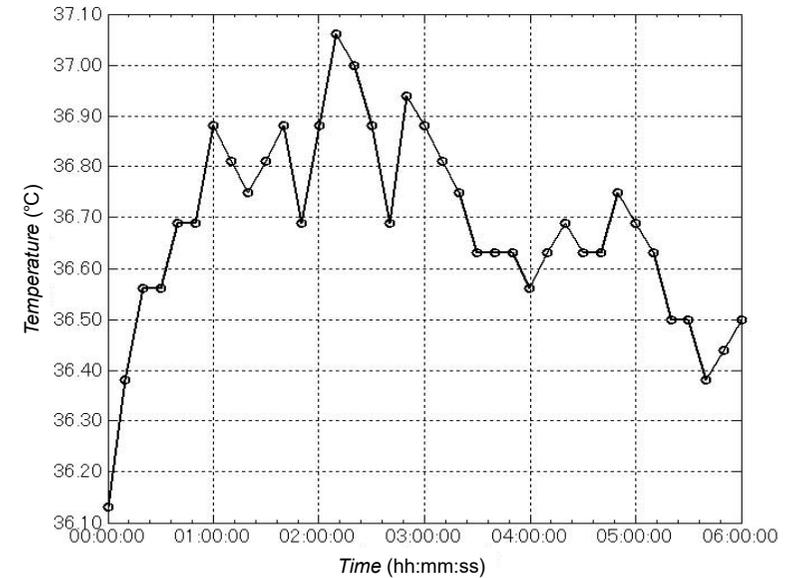
Measurement Sites

1. Sublingual space
2. Axilla
3. Groin
4. Neck
5. Rectum
6. Esophagus
7. Tympanum
8. External auditory canal
9. Tympanum by non-contact thermometer
10. Nasal cavity
11. Bladder
12. Urine
13. Digestive tract by radio capsule
14. Thorax by zero-heat-flow thermometer
15. Forehead by zero-heat-flow thermometer



5

Body Temperature during Sleep



6

Mercury Thermometer

German physicist Daniel Gabriel Fahrenheit in 1724



Length of the mercury within the tube varies nearly linearly according to temperature of the mercury.

Capillary

Narrow bore

Surface tension prevents mercury from flowing back the bulb through narrow bore.

Calibrate marks

Mercury volume

Bulb

Sublingual temperature

7

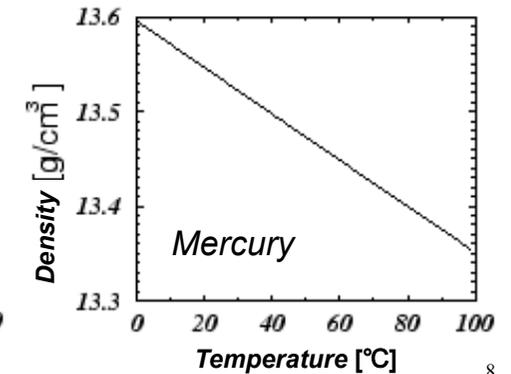
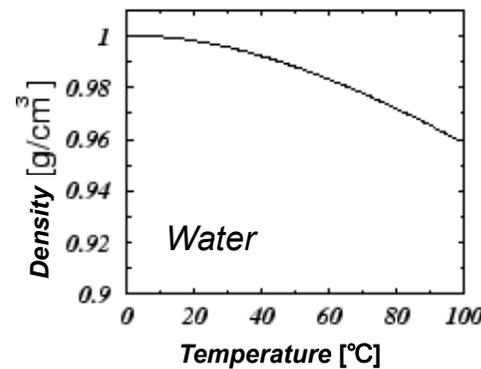
Thermal Dilatability

When mercury gets warmer it expands.

This increase in volume is measured by the scale on a mercury thermometer.

$$\alpha(T, p) = \frac{1}{V} \left(\frac{\partial V}{\partial T} \right)_p \quad \frac{\Delta V}{V} = - \frac{\Delta \rho}{\rho} \quad \alpha(T, p) = - \frac{1}{\rho} \left(\frac{\partial \rho}{\partial T} \right)_p$$

α : temperature coefficient



8

Thermoresistive Elements

Temperature coefficient: $\alpha = \frac{1}{R} \frac{dR}{dT}$

band gap energy of the semiconductor

Resistivity: $\rho \propto \exp\left(\frac{E_g}{2kT}\right)$

Boltzmann constant

A thermistor has relatively higher resolution and larger temperature coefficient, typically about -0.04/K

Material	Temp. Coeff. (K ⁻¹)	Resistivity (Ωm)
Platinum	3.9×10^{-3}	10×10^{-8}
Nickel	6.7×10^{-3}	6.8×10^{-8}
Aluminum	4.2×10^{-3}	2.7×10^{-8}
Tungsten	5.3×10^{-3}	5.5×10^{-8}

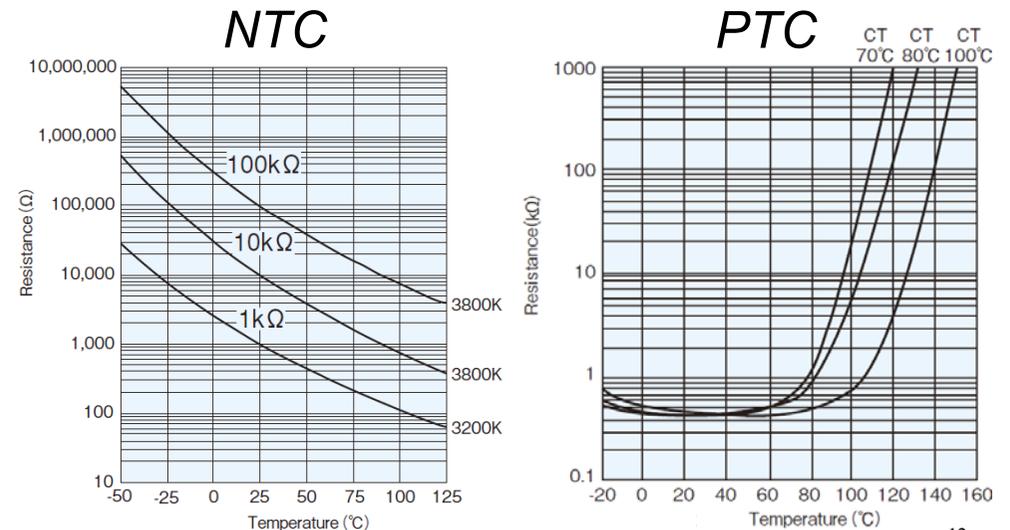
NTC and PTC Thermistors

- Thermally sensitive resistor
 - Electrical resistance is sensitive to temperature change
 - Metal oxide such as iron, nickel, cobalt, manganese, copper, 2~4 mixture, molded into various shapes at 1200~1500°C
- Measurement range = -50~350°C
- NTC (Negative Temperature Coefficient)
 - Inverse proportional relation between temperature change and resistance change
- PTC (Positive Temperature Coefficient)
 - proportional relation between temperature change and resistance change

Significant Features

- High sensitivity
 - Larger resistor-temperature coefficient = -2.8~-5.1%/°C
- Easy fabrication
 - Various shapes, miniaturization available
- Wide range of selectable resistor value
 - Tens of Ω~several hundreds kΩ

Characteristic Curves



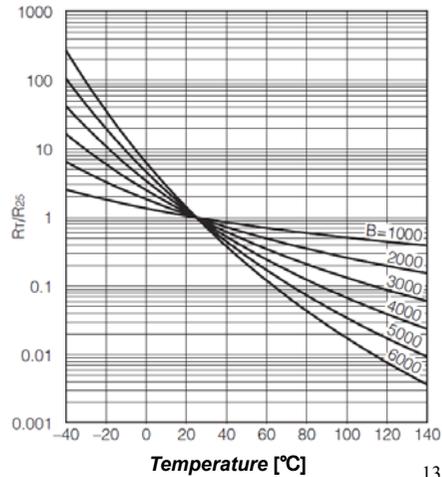
Temperature Coefficient

- T_0 : reference temperature, usually 298.15K (25°C)
- R_0 : resistance at T_0
- B : thermistor constant
 $=E_g/2k=1500\sim 6000K$

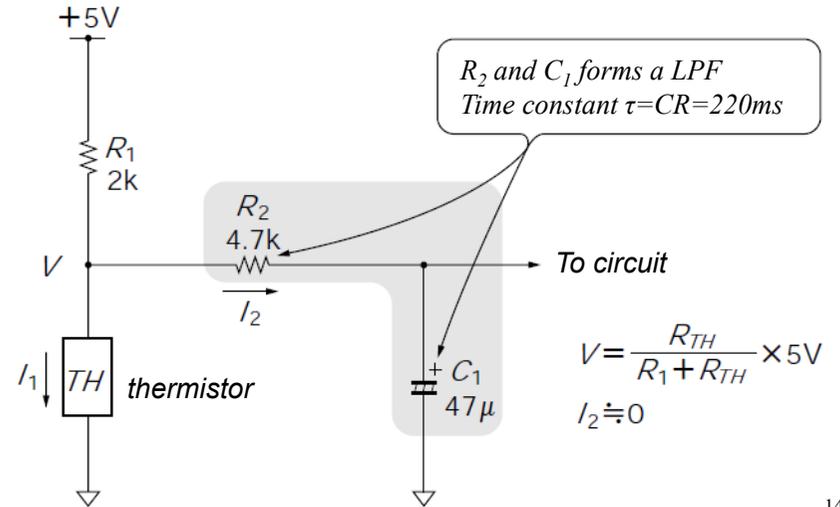
$$R(T) = R_0 \exp \left[B \left(\frac{1}{T} - \frac{1}{T_0} \right) \right]$$

- α : temperature coefficient

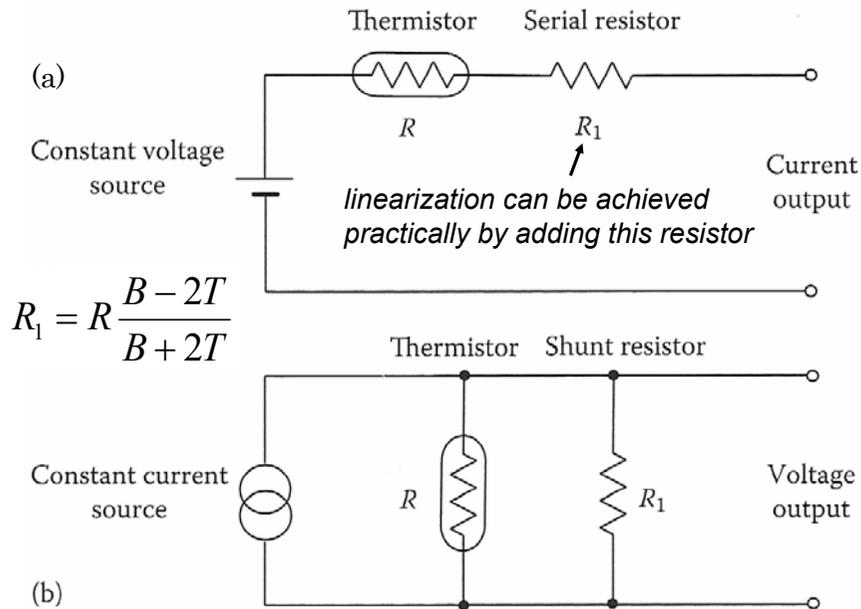
$$\alpha = \frac{1}{R} \frac{dR}{dT} = \frac{d}{dT} \left(\frac{B}{T} \right) = -\frac{B}{T^2}$$



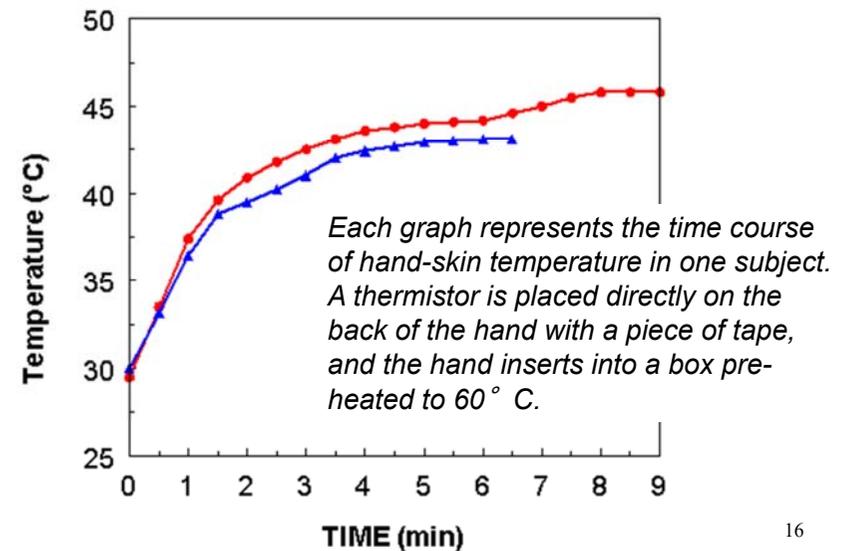
Temperature-Voltage Converter



Linearization Circuits



Thermistor Output vs. Time



Two Measurement Methods

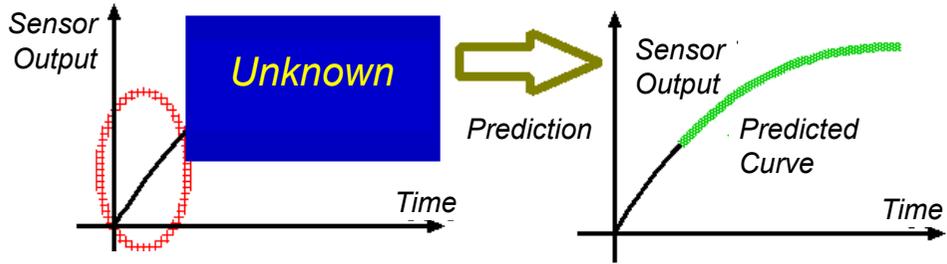
Direct method

Real temperature measurement is complete at the time of the sensor equal to the body temperature (axilla \approx 10 min, mouth \approx 5 min)

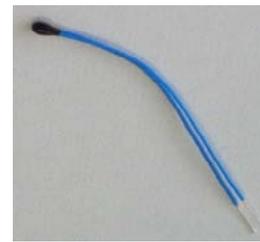
Predictive method

Using an empirical curve, predict the final temperature value from the first 1 min or several tens of sec real measurement.

10 minutes later...

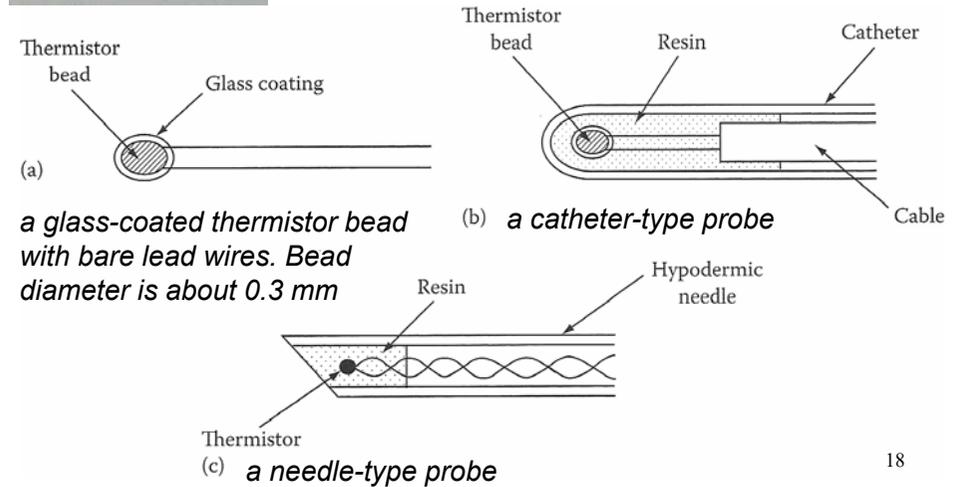


First 1 min real measurement



Thermistor Probes

the thermistor is connected to a flexible insulated cable, and the connected part is also insulated and completely waterproof



(a) a glass-coated thermistor bead with bare lead wires. Bead diameter is about 0.3 mm

(b) a catheter-type probe

(c) a needle-type probe

Electronic Thermometers

Basal thermometer

Range 32.00°C~42.00°C

Accuracy $\pm 0.05^\circ\text{C}$ (35.00~38.00°C)

$\pm 0.1^\circ\text{C}$ (32.00~34.99°C, 38.01~42.00°C)



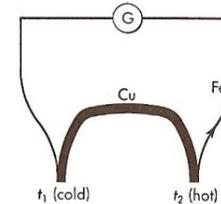
Medical thermometer

Range 32.0°C~42.0°C

Accuracy $\pm 0.1^\circ\text{C}$

BBT increases 0.3~0.5°C in ovulation day and shifts from low temperature to high temperature

Seebeck effect = a temperature difference between two dissimilar electrical conductors or semiconductors produces a voltage difference between the two substances.

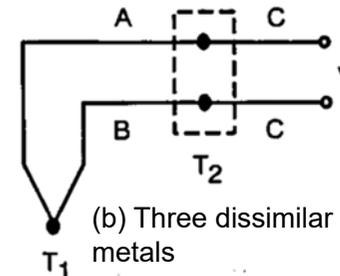


Sensitivity between 20°C to 40°C:

41 $\mu\text{V/K}$ for copper/constantan

40 $\mu\text{V/K}$ for chromel/alumel

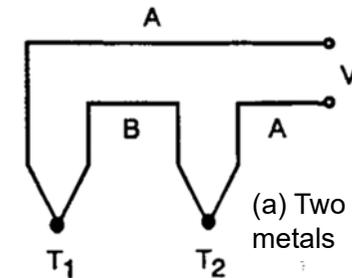
6.1 $\mu\text{V/K}$ for platinum/rhodium



(b) Three dissimilar metals

Thermocouple

thermoelectric sensor



(a) Two dissimilar metals

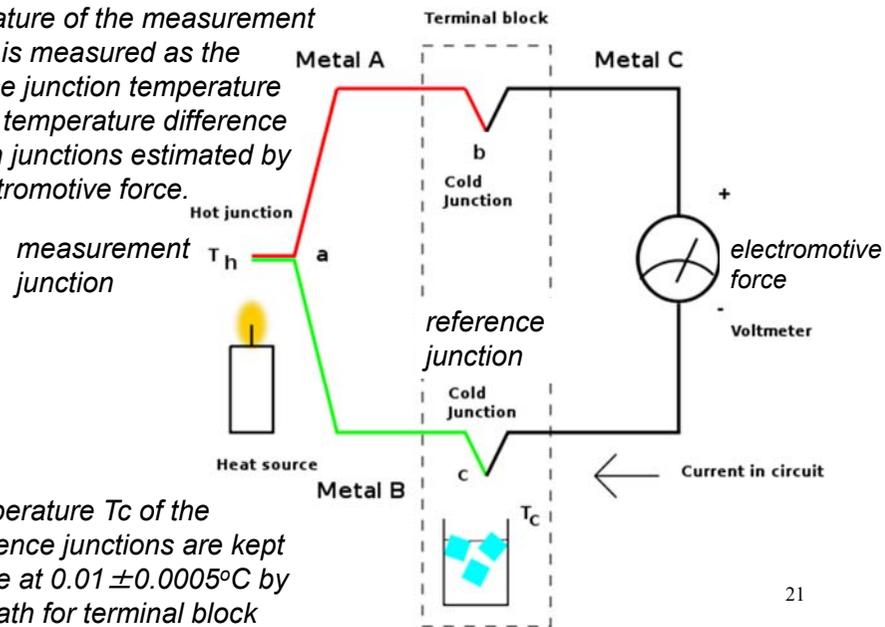
Electromotive force depends on the **temperature difference** between two **junctions**

When the temperature of the reference junction T_2 is kept constant, electromotive force V varies only with the temperature of the measurement junction T_1

a third metal C is connected to both metals A and B , and as long as two new junctions are at the same temperature, it provides the same electromotive force as that of the (a), regardless of the material of the third metal.

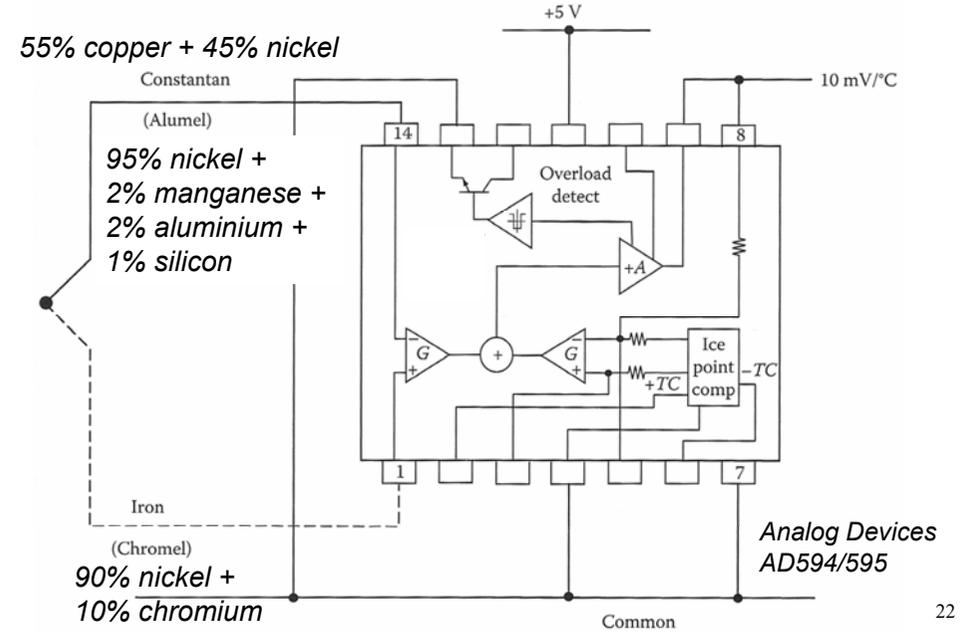
Thermocouple Circuit

Temperature of the measurement junction is measured as the reference junction temperature plus the temperature difference between junctions estimated by the electromotive force.



Temperature T_c of the reference junctions are kept stable at $0.01 \pm 0.0005^\circ\text{C}$ by ice bath for terminal block

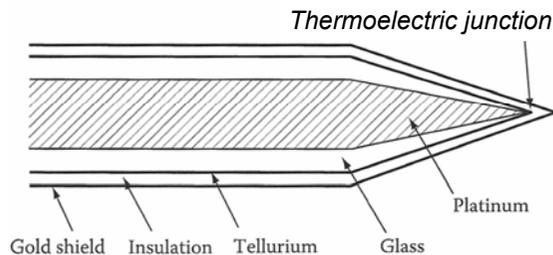
Thermocouple IC



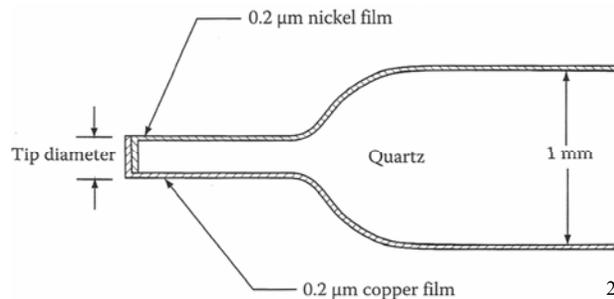
Micro Thermocouple

local temperature measurement

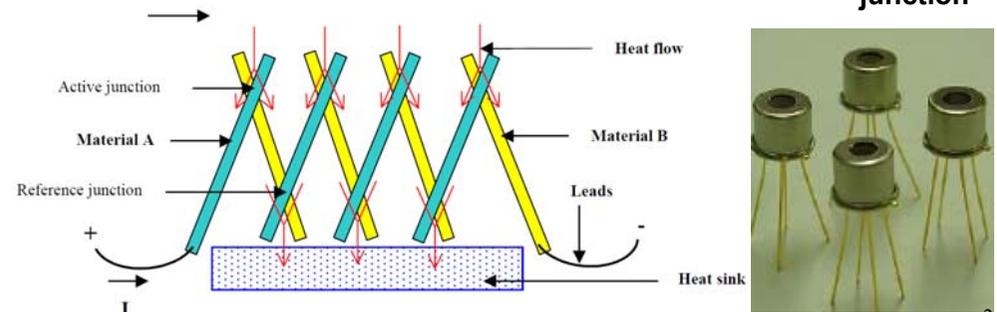
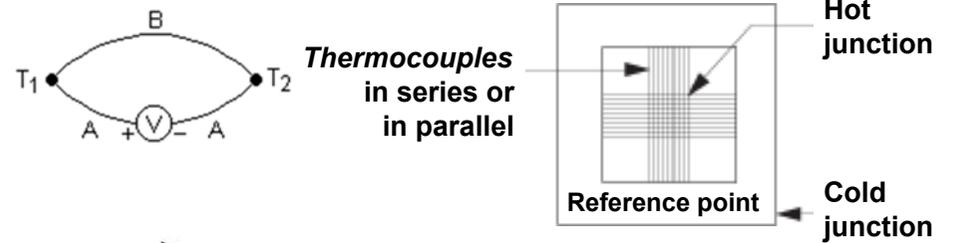
Junction is about 1 μm , made of glass-coated microelectrodes. a tip of thin platinum wire 25 μm in diameter was tapered, and a thin glass coating on the platinum was made leaving an exposed cone of platinum. A thin film of tellurium was formed, insulated by coating with a thin film of negative photoresist, and finally a gold film was formed to shield it from electromagnetic interference.



A quartz rod was tapered to form a tip of about 10 μm in diameter. A nickel layer was vacuum deposited on one side and a copper layer on the other, with two metals overlapping only at the tip end. Finally, the probe was coated with polymer for insulation.



Thermopile



The voltage V across a **p-n junction** at constant forward-bias current has **linear dependency** on the absolute temperature T .

Any diode or transistor can be a temperature sensor.

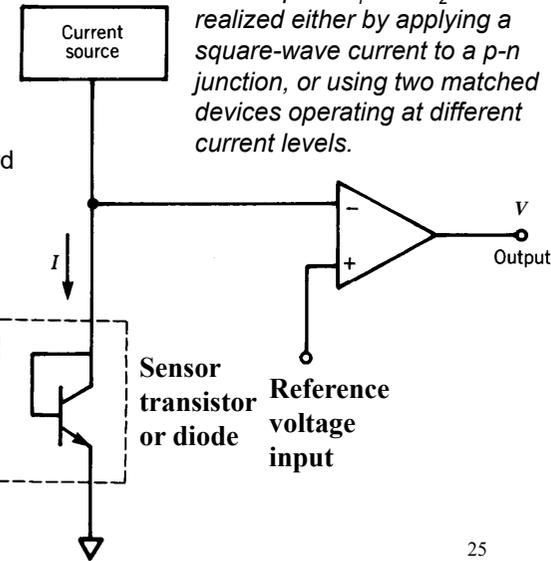
$$I = Ae^{\frac{qV - E_g}{kT}}$$

If the p-n junction in a diode or transistor is driven by different forward current levels I_1 and I_2 , and voltages V_1 and V_2 are developed at these current levels

$$V_1 - V_2 = \frac{kT}{q} \ln \frac{I_1}{I_2}$$

- I = forward bias current
- A = constant depending on the geometry of the junction
- q = electron charge
- V = voltage across the junction
- E_g = band gap energy
- k = Boltzmann constant
- T = absolute temperature

p-n Junction Sensor



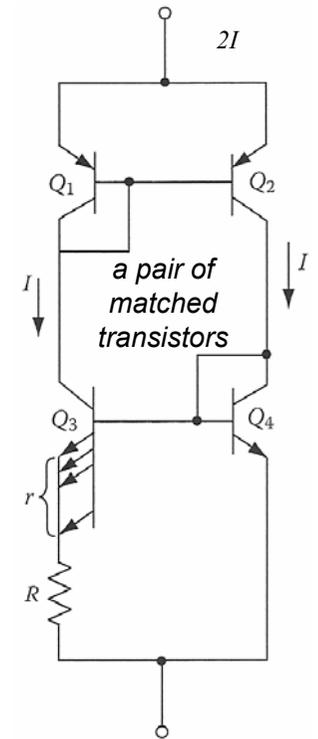
25

Two-terminal Current-output Sensor

If transistors Q_1 and Q_2 are assumed to be equal and have a large gain, their collector currents are equal and constrain the collector current of Q_3 and Q_4 . Q_3 has r base-emitter junctions, and each one is identical to that of Q_4 .

- I = forward bias current
- R = bias resistor
- q = electron charge
- r = number of base-emitter junctions
- k = Boltzmann constant
- T = absolute temperature

$$V = R \cdot I = \frac{kT}{q} \ln r$$



26

Infrared Radiometer

thermal radiation power emitted from the human body is used to measure human body temperature

total power that enters the thermometer

$$W = \epsilon P(T_s) + (1 - \epsilon)P(T_a)$$

ϵ : emissivity

Emission component $\epsilon P(T_s)$

Reflection component $(1 - \epsilon)P(T_a)$

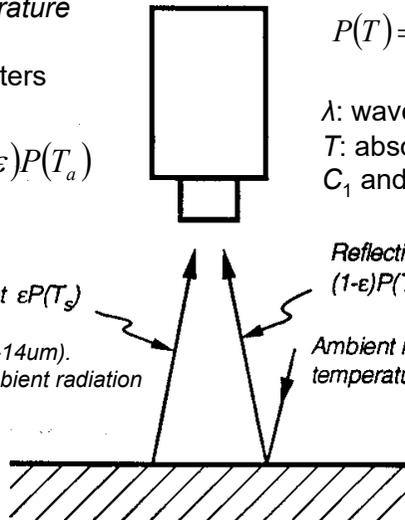
skin emissivity ≈ 0.97 (8-14 μ m).
3% of reflection from ambient radiation

Object surface temperature T_s

- λ : wavelength
- T : absolute temperature
- C_1 and C_2 : universal constants

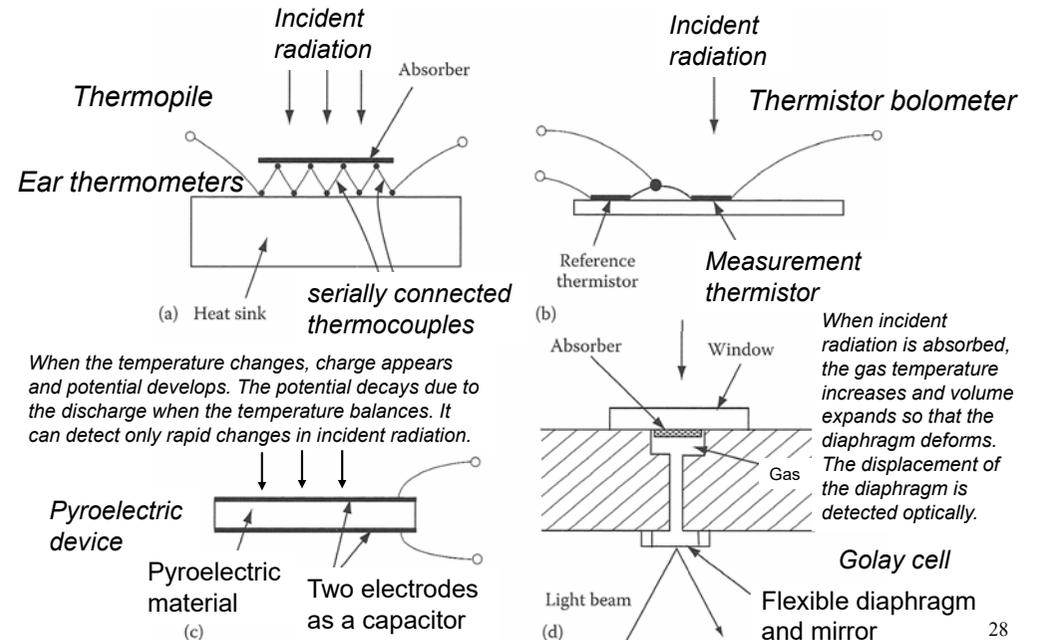
Planck's radiation formula

$$P(T) = \int \frac{C_1 \lambda^{-5}}{\exp(C_2 / \lambda T) - 1} d\lambda$$



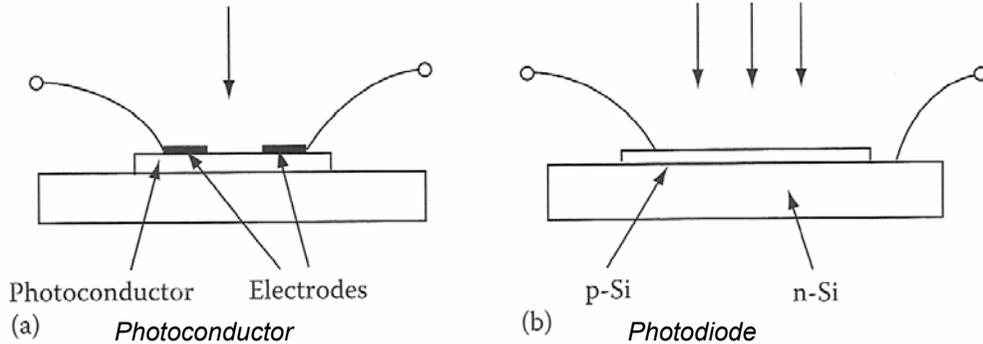
27

Thermal Detectors



28

Photon Detectors



(a) **Photoconductor**

Carriers that are electron-hole pairs are generated by incident photons when the photon energy exceeds the band gap energy. Generated carriers create a photo current when a potential is applied externally. Carriers are also generated by thermal energy and this results in a dark current in the entire frequency range. Dark current can be reduced by cooling the detector.

(b) **Photodiode**

A p-n junction operated under reverse bias. At the boundary of the p and n region, there is a depletion region where carrier density is zero. When an electron-hole pair is generated in a depletion region by an incident photon, the electron and hole are separated and generate an electric current in the external circuit.

Infrared Skin Thermometer

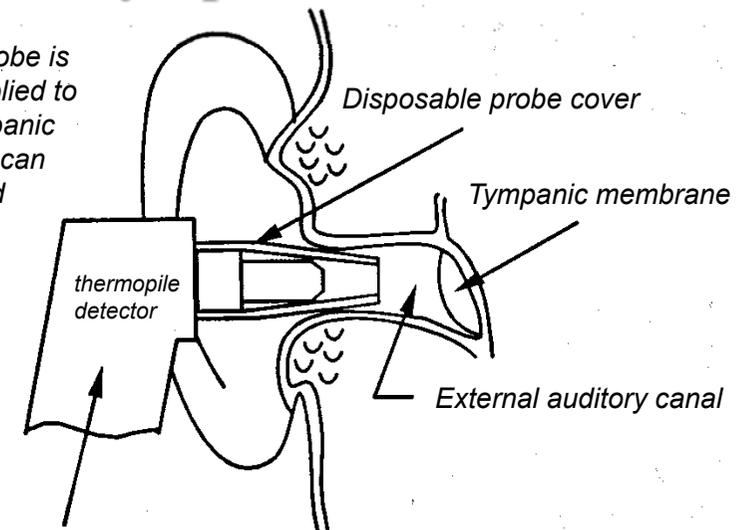


Infrared Tympanic Thermometer



Infrared Tympanic Thermometer

When the probe is correctly applied to the ear, tympanic temperature can be measured within 2 sec.



Tympanic thermometer probe

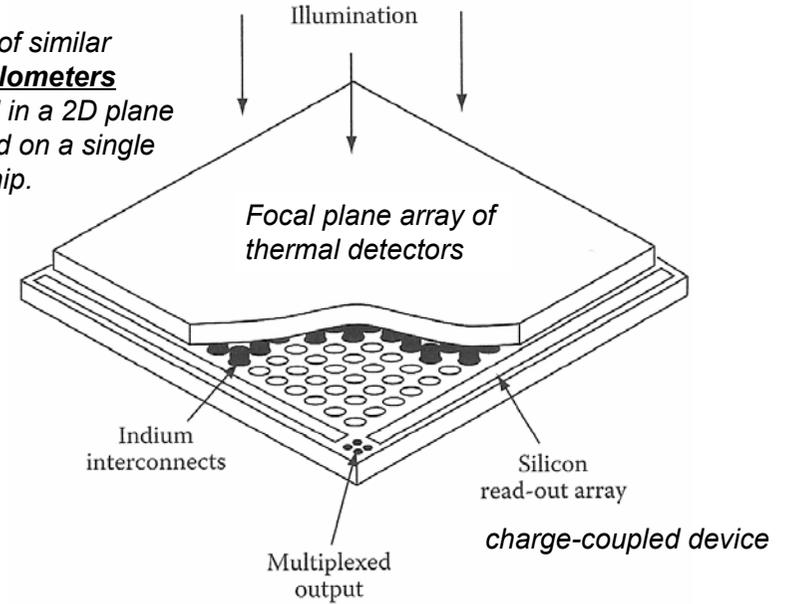
Thermo Mirror

It captures the temperature via a built-in infrared sensor in a mirror.
By looking at the mirror and your temperature will be measured automatically.



Infrared Image Device

A matrix of similar **microbolometers** arranged in a 2D plane fabricated on a single silicon chip.



Thermo Camera

Infrared thermography provides thermal images by thermo camera. It realizes a noncontact measurement.

To obtain a thermal image of an object, surface temperature at many points on the object should be measured.

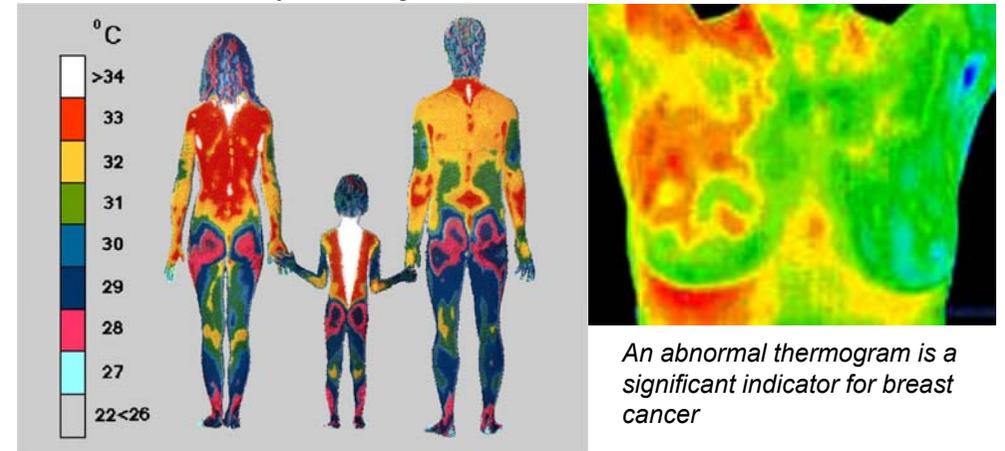


This is achieved by either mechanical scanning by means of moving mirrors or prisms, or by electronic scanning of the infrared detectors placed at the focal plane.

Raytheon, Radiance MS

Thermogram and Breast Cancer

Whole Body Thermogram



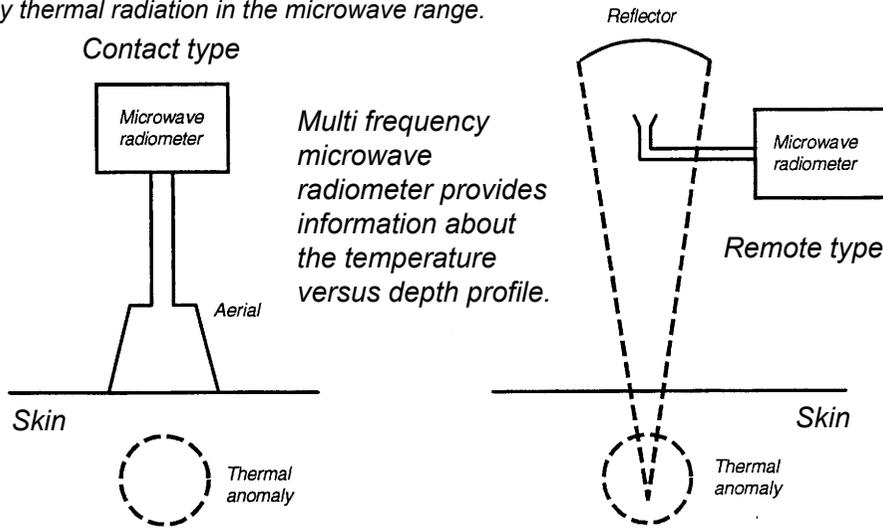
An abnormal thermogram is a significant indicator for breast cancer

A major mechanism involved with all degenerative disease is inflammation. Inflammation is present in precancerous and cancerous cells, in torn muscles, ligaments and arthritic joints. Heat is an indication of inflammation. Thermography measures inflammation and deficiencies in the body due to various dysfunctions such as diabetes, heart disease and some cancers.

Microwave Thermometer

Active microwave imaging method estimates local temperatures in the body from a reconstructed image of the temperature-dependent dielectric constant of the tissue.

Passive microwave imaging method obtains thermal images from the deep tissue by thermal radiation in the microwave range.



37

the amount of heat that passes through the plate per unit time and unit area

Heat Flow Measurement

$$\text{heat flow } Q = k\Delta T/d$$

k : thermal conductivity

d : thickness of the plate

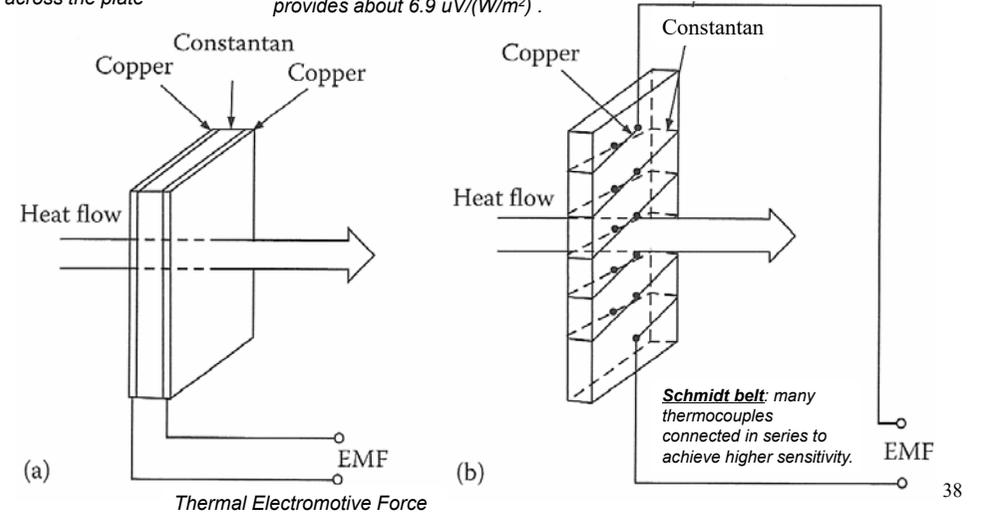
ΔT : temperature difference across the plate

a constantan plate of 5 mm is coated by copper on both sides, its sensitivity is only about $0.083 \mu\text{V}/(\text{W}/\text{m}^2)$.

a tellurium-silver alloy of 1.5 mm coated on its two sides with copper provides about $6.9 \mu\text{V}/(\text{W}/\text{m}^2)$.

estimate heat loss from the body, or efficiency of thermal insulation of clothes or animal fur

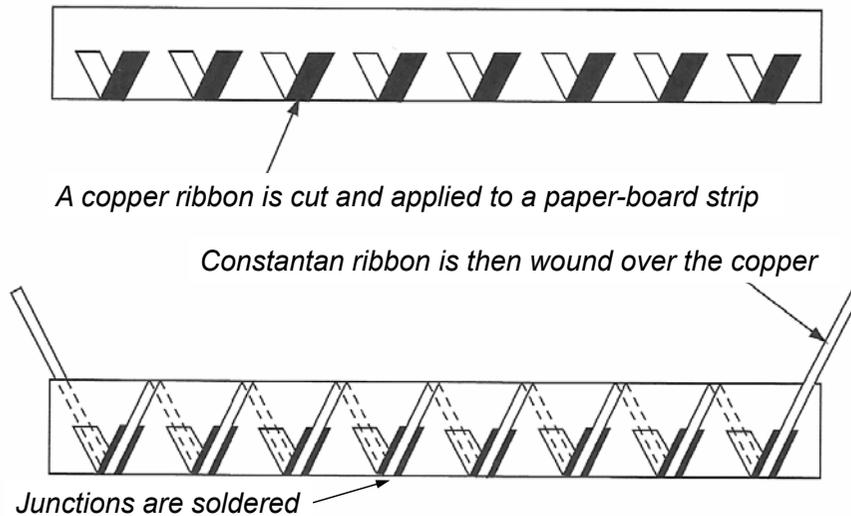
thermocouple wire is wound spirally on a strip having adequate thermal resistance, so that every half-turn of each spiral consists of constantan wire, and the other half-turn consists of copper wire.



38

Schmidt-belt Heat Flow Sensor

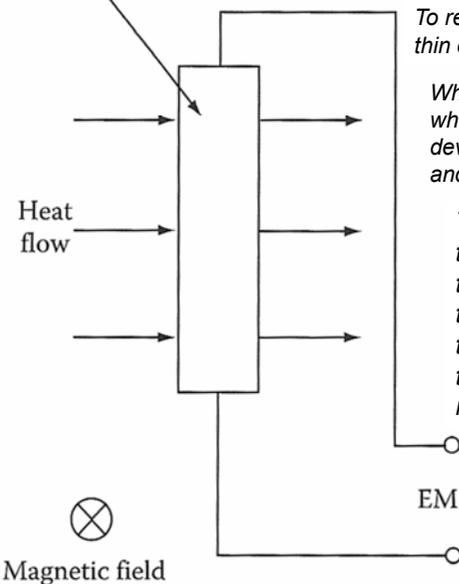
Copper and constantan ribbons are connected in parallel at every half-turn, and thus loop current may be generated if a temperature gradient along this half-turn is developed.



39

Nernst Effect Principle

Semiconductor



When a heat flow sensor is attached to the object surface, natural heat flow distribution may be disturbed. To reduce this effect, the heat flow sensor should be thin enough → **transverse thermomagnetic** technique

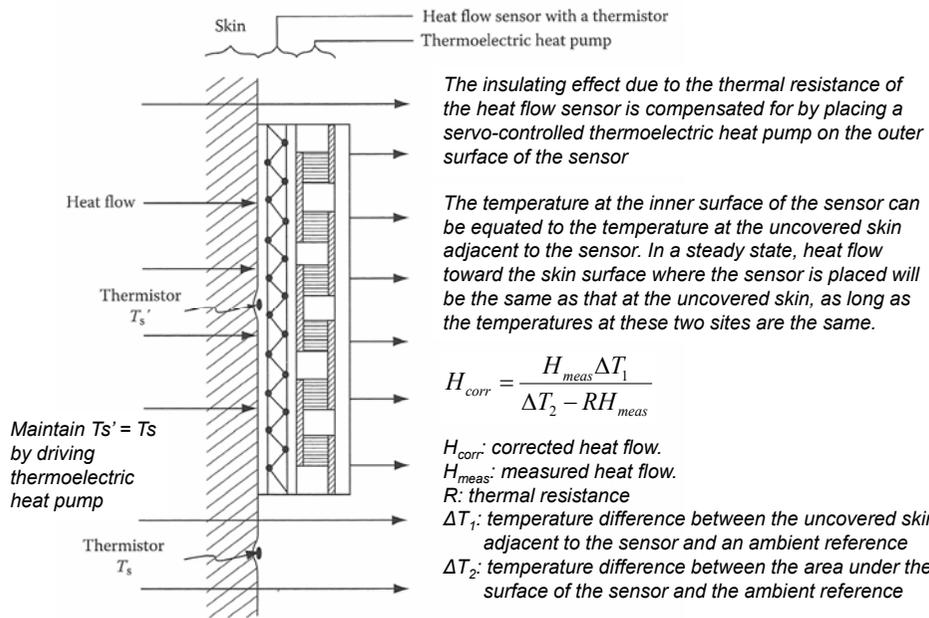
When heat flows through a semiconductor plate to which a transverse magnetic field is applied, EMF is developed perpendicular to the direction of heat flow and the magnetic field.

The advantage of using the Nernst effect is that the output EMF is proportional not to the temperature difference but to the temperature gradient. For a given heat flow, the temperature gradient is independent of the thickness, so thermal resistance can be reduced without reducing sensitivity.

The disadvantage of using an external magnetic field is that this limits most applications of this technique, thus is used only in thermal radiation detectors

40

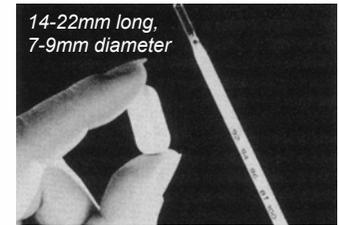
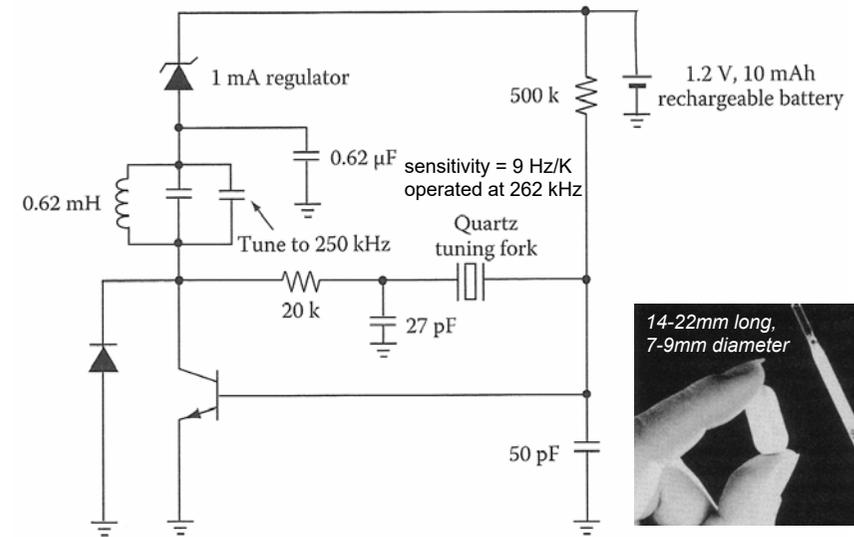
Body Surface Measurement



41

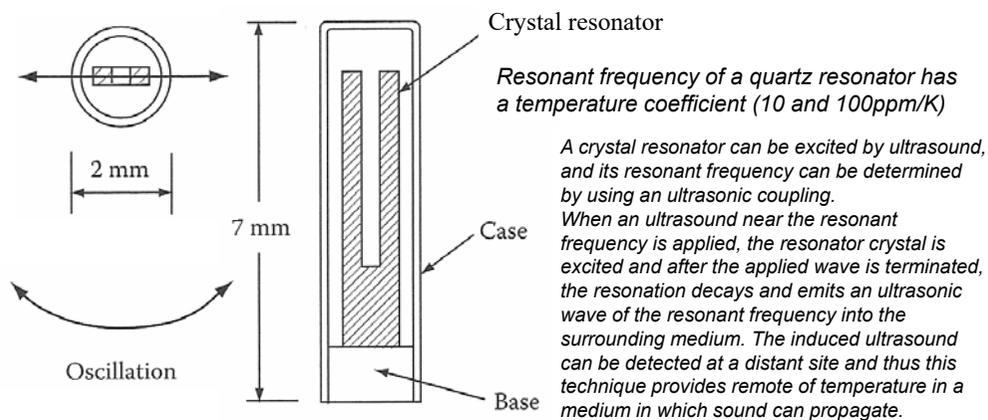
body core temperature in the digestive tract

Swallowable Capsule



42

Quartz Crystal Resonator

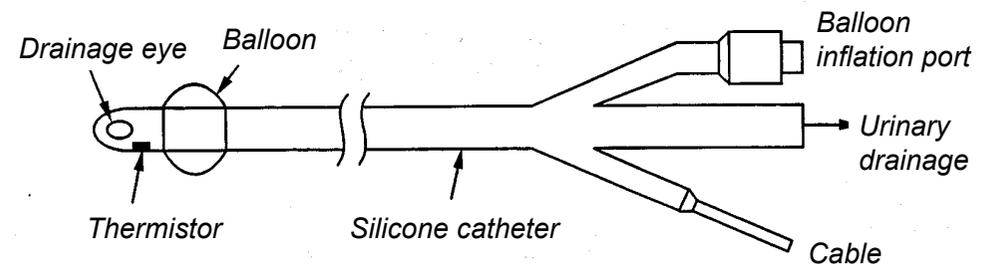


Its resonant frequency is about 40kHz with a temperature coefficient of about 3.2Hz/K. To measure temperature, the resonator is excited for about 0.4 s by applying an ultrasonic wave near the resonant frequency.

The damped oscillations in the resonant frequency are measured. The absolute accuracy is about 0.1°C, with temperature resolution about 0.01°C. It has been shown that when the capsule is swallowed, temperature measurements can be performed from the abdominal skin surface.

43

Thermistor-tipped Foley's Bladder Catheter

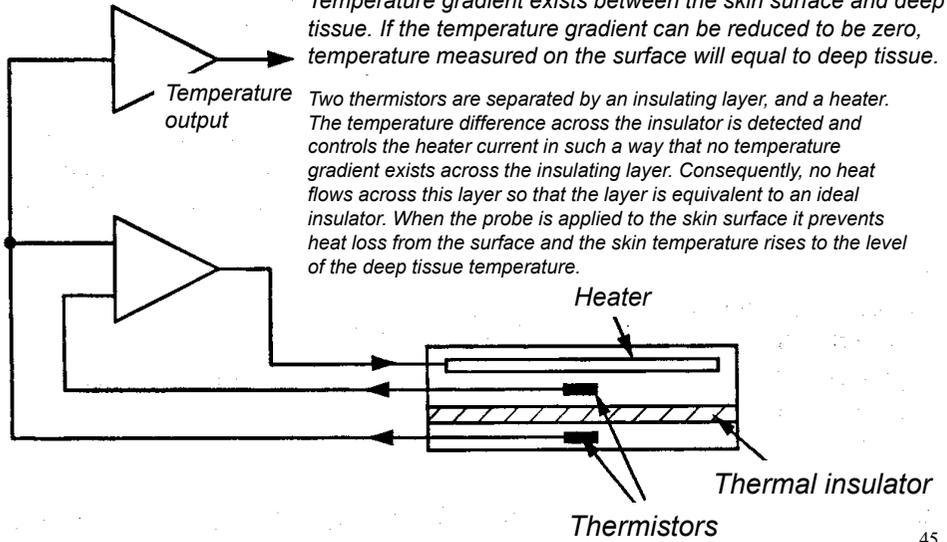


44

Body core temperature is monitored at deeper sites of the body such as the rectum, esophagus, and bladder using **indwelling thermometer probes**.

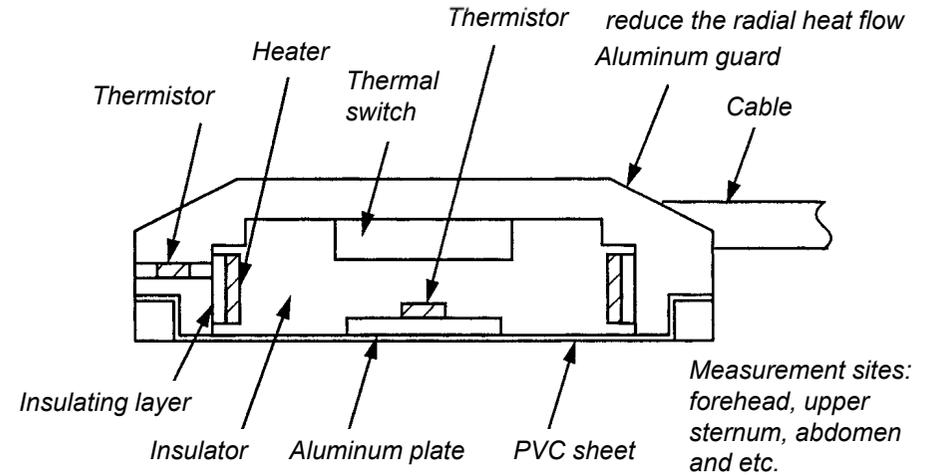
Zero-heat-flow Thermometer

measurement of deep body temperature **from the skin surface**



45

Zero-heat-flow Probe

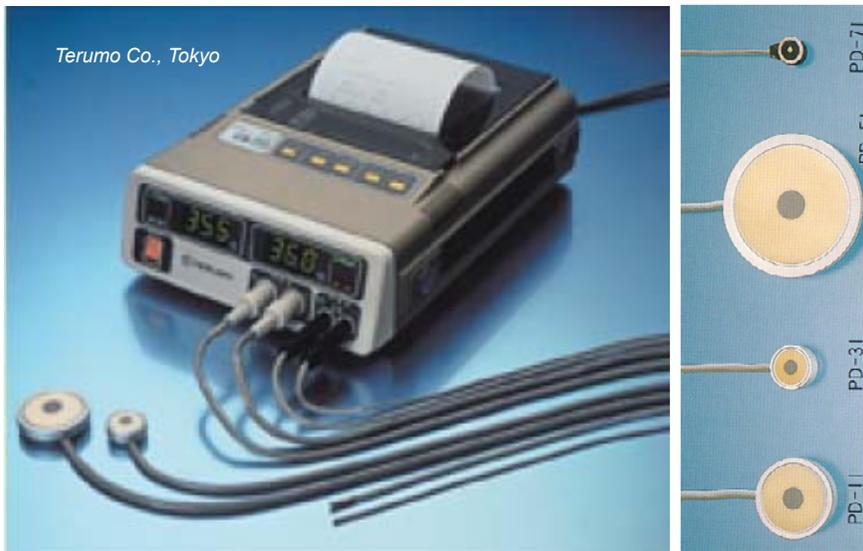


The initial response time when the probe is applied to the exposed skin is 15 to 20min. After thermal equilibrium is reached, the probe temperature follows physiological changes in core temperature.

46

Deep Body Thermometer

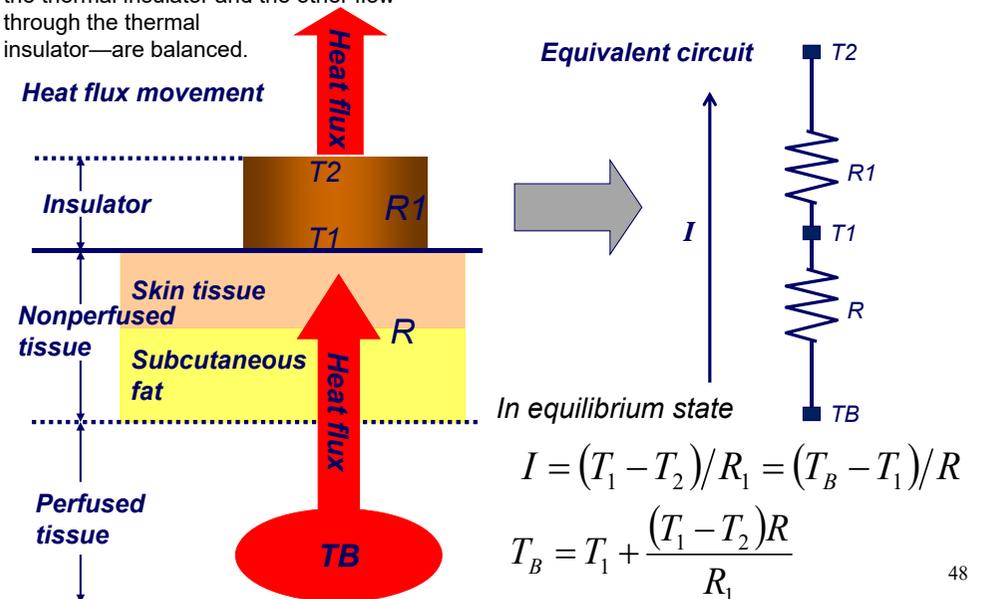
1.5 to 8 cm in diameter



47

when the body surface is covered with a thermal insulator and the temperature reaches equilibrium, two heat fluxes—one flow from the deep body tissue to the body surface beneath the thermal insulator and the other flow through the thermal insulator—are balanced.

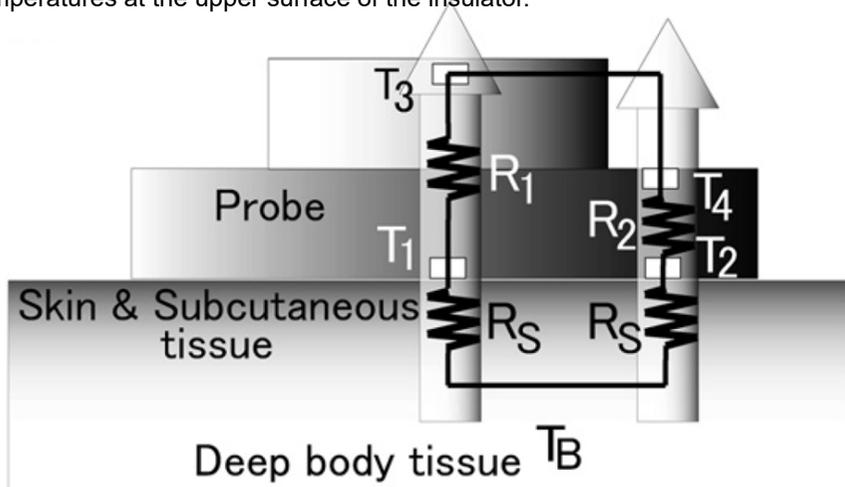
Heat Flux Model



48

Dual-Heat-Flux Circuit Model

Body surface is covered with 2 kinds of heat insulators with thermal resistances R_1 and R_2 .
 R_S is the thermal resistance of the skin and subcutaneous tissue;
 T_1 and T_2 are the skin temperatures beneath the insulator, and T_3 and T_4 are the temperatures at the upper surface of the insulator.



Estimation of Deep Temperature

$$T_B = T_1 + \frac{(T_1 - T_3)R_S}{R_1} \quad T_B = T_2 + \frac{(T_2 - T_4)R_S}{R_2}$$

Suppose both R_s identical

Define $K=R_1/R_2$ to describe sensor property

When the ratio of the thermal resistance K is obtained, we can get the deep body temperature T_B from T_1-T_4

$$T_B = T_1 + \frac{(T_1 - T_2)(T_1 - T_3)}{K(T_2 - T_4) - (T_1 - T_3)}$$

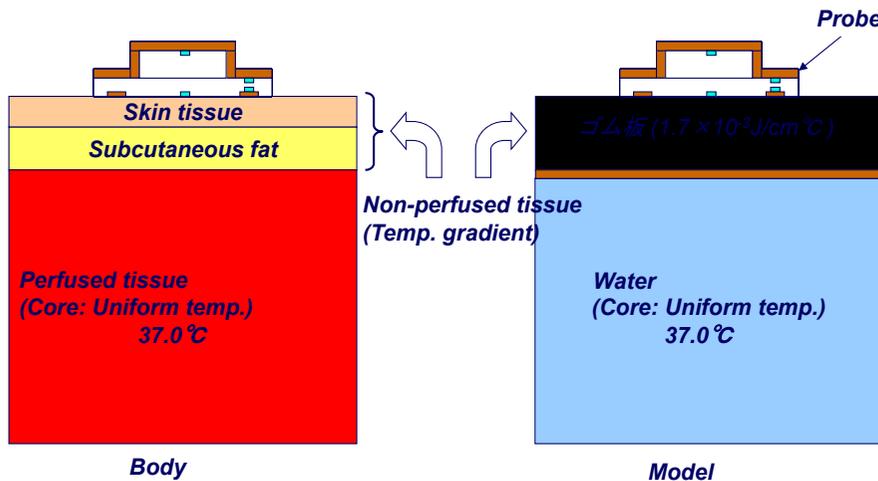
K is obtained by a simulation experiment.

$$K = \frac{(T_B - T_2)(T_1 - T_3)}{(T_B - T_1)(T_2 - T_4)}$$

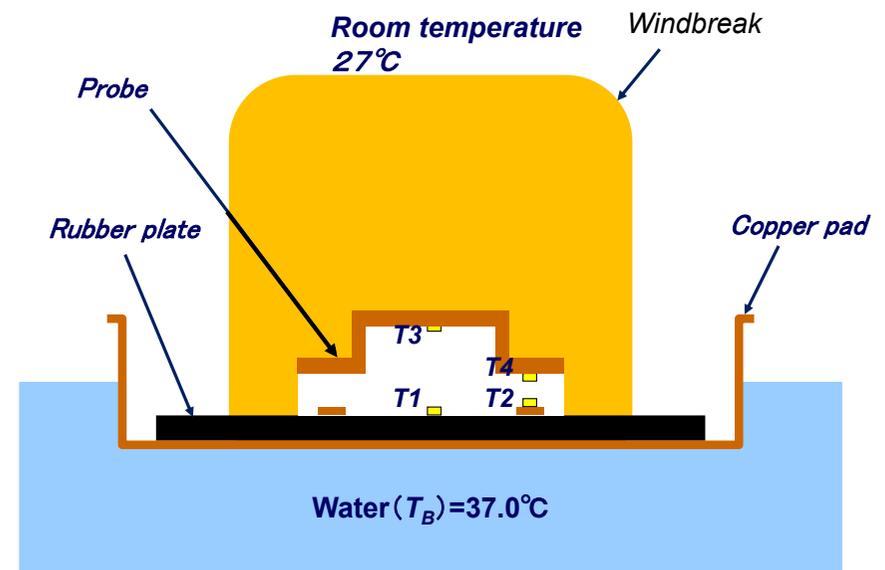
Estimation of K Value

$$K = \frac{(T_B - T_2)(T_1 - T_3)}{(T_B - T_1)(T_2 - T_4)}$$

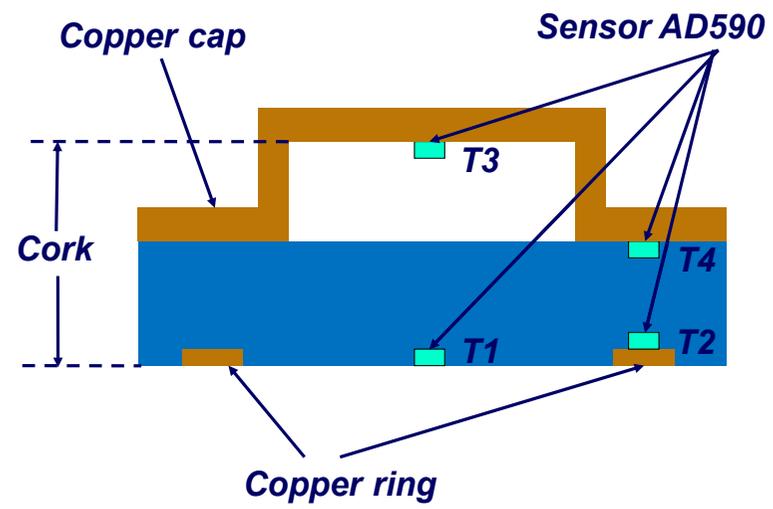
The probe is set on a rubber sheet that is placed over the inner bottom of a copper vat floating in a water bath where temperature T_B is known. In equilibrium state, T_1-T_4 are measured.



Simulation Model



Probe Structure



53

Probe Prototype



54